

CWT IN BIOMEDICAL  
IMAGE DENOISING

E. Hošťálková, A. Procházka

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# COMPLEX WAVELET TRANSFORM IN BIOMEDICAL IMAGE DENOISING

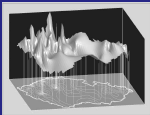
Eva Hošťálková & Aleš Procházka

Institute of Chemical Technology in Prague  
Dept of Computing and Control Engineering  
<http://dsp.vscht.cz/>



**ICT PRAGUE**

Technical Computing Prague 2007



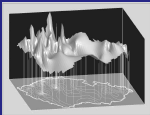
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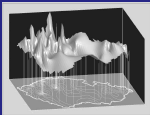
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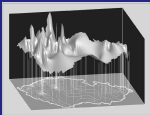
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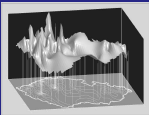
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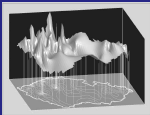
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## Applications of the Wavelet Transform in Image processing

- Noise reduction
- Image compression and coding
- Edge detection
- Feature extraction  $\Rightarrow$  segmentation & retrieval
- Restoration of missing or corrupted components

## Limitations of the Discrete Wavelet Transform (DWT)

- Zero crossings of the coefficients at a singularity
- Strong shift dependence
- Aliasing  $\Leftarrow$  downsampling and non-ideal filters
- Lack of directional selectivity - unable to distinguish between  $+45^\circ$  and  $-45^\circ$



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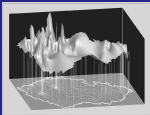
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## Undecimated DWT

- DWT without downsampling.

### ADVANTAGES

- Shift independence

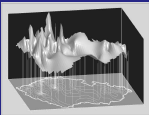
### DISADVANTAGES

- Poor directional selectivity
- Great computation cost

## Complex Wavelet Transform (CWT)

- Employs analytic complex wavelets
- $\Rightarrow$  Magnitude-phase representation
  - Large magnitude  $\Rightarrow$  presence of a singularity
  - Phase: its position within the support of the wavelet
- $\Rightarrow$  Shift invariance & no aliasing
- In this work: Dual-Tree CWT (DTCWT) by Kingsbury, Selesnick





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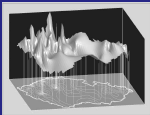
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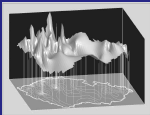
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## Dual Tree Complex Wavelet Transform

- Dual tree (two DWT trees) of real filters  $\Rightarrow$  real and imaginary parts of each complex coefficient
- Perfect reconstruction (PR)
- Approx. analytic filters  $\Rightarrow$  approx. shift invariance
- Directional selectivity in 2D:

### DTCWT

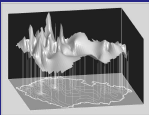
- 6 directional subbands
- $\pm 15^\circ$ ,  $\pm 45^\circ$  and  $\pm 75^\circ$

### DWT

- 3 directional subbands
  - $0^\circ$ ,  $45^\circ$  and  $90^\circ$
- Limited redundancy  $2^d$  in  $d$ -dimensional space

## Q-Shift DTCWT

- By Prof. Kingsbury, used in this work
- Q-shift ... quarter of a sample period shift



# Introduction to DTCWT

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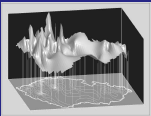
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## Directional Selectivity of 2D Wavelets

(a) REAL PARTS OF 2D Q-SHIFT COMPLEX WAVELETS



+15°

+45°

+75°

-75°

-45°

-15°

(b) IMAGINARY PARTS OF 2D Q-SHIFT COMPLEX WAVELETS



+15°

+45°

+75°

-75°

-45°

-15°

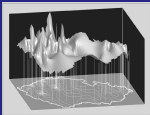
(c) 2D DB4 REAL WAVELETS



90° (*LoHi*)

45° (*HiHi*)

0° (*HiLo*)



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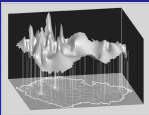
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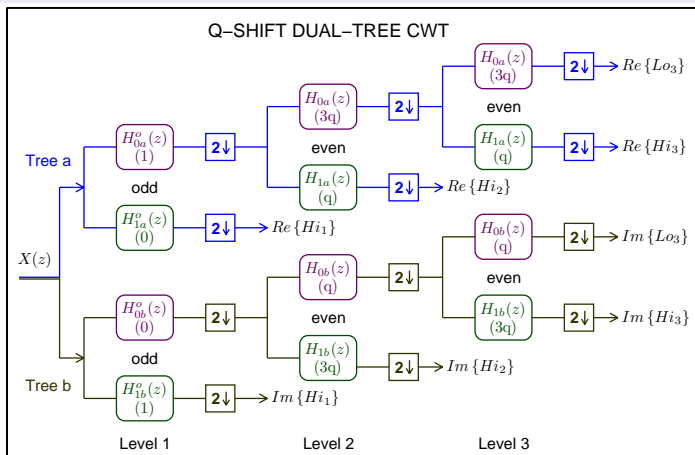
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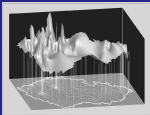
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## Q-Shift DTCWT 3-level analysis scheme



Red - lowpass filters, green - highpass filters,  $2\downarrow$  - downsampling by 2



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## Q-Shift DTCWT

- Level 1: any orthogonal/biorthogonal set of filters
- Beyond level 1: even-tap Q-shift filters
- Both trees - same frequency response
- Conjugate symmetry  $\Rightarrow$  linear phase
- Individual asymmetry  $\Rightarrow$  orthonormal PR

## Orthonormal Set of Q-Shift Filters

- Filters in tree  $b$  - reverse of the filters in tree  $a$

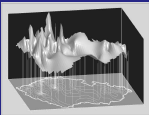
$$h_{0b}(n) = h_{0a}(N-1-n)$$

- Synthesis filters - reverse of the analysis filters

$$g_{0a}(n) = h_{0a}(N-1-n)$$

where  $n = 0, \dots, N-1$  and  $N$  is the filter length





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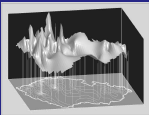
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## Analytic Wavelets

- Complex wavelet  $\psi_c(t) = \psi_r(t) + j \cdot \psi_i(t)$  is **analytic** when

$$\psi_i(t) = HT\{\psi_r(t)\} = \frac{1}{\pi} \int_{-\infty}^{\infty} \frac{\psi_r(\tau)}{t-\tau} d\tau = \psi_r(t) \frac{1}{\pi t}$$

where  $t, \tau$  is continuous time

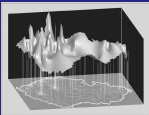
- Fourier transform of a Hilbert transform pair

$$H_i(\omega) = FT\{HT\{\psi_r(t)\}\} = -j \cdot \text{sgn}(\omega) H_r(\omega)$$

where  $\omega$  denotes frequency and  $j$  the complex unit

## Implications

- Single sided spectrum  $\Rightarrow$  no aliasing  $\Rightarrow$  shift invariance
- Impossible with compact support!  $\Rightarrow$  only approximately analytic



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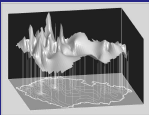
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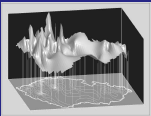
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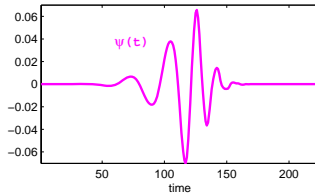
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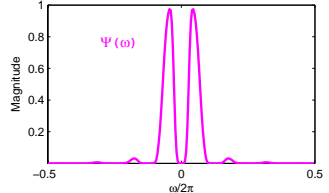
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## Frequency Spectra of a Real and an Analytic Wavelet

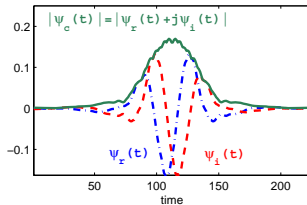
(a) Db-7 REAL WAVELET



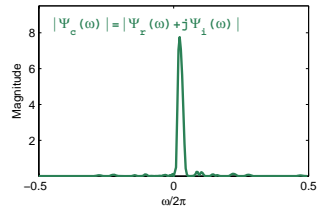
(b) Db-7 WAVELET: DFT



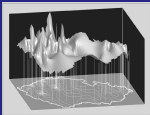
(c) Q-SHIFT COMPLEX WAVELET



(d) Q-SHIFT WAVELET: DFT



4 levels, 14-tap filters: Daubechies for DWT and q-shift for DTCWT.



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## Half-Sample Delay Condition

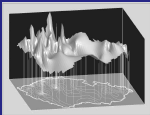
- Half of a sample period difference between filters in tree  $a$  and  $b \Rightarrow$  analytic
- In the Fourier domain:

$$\text{MAGNITUDE } |H_{0b}(e^{j\omega})| = |H_{0a}(e^{j\omega})|$$

$$\text{PHASE } \angle H_{0b}(e^{j\omega}) = \angle H_{0a}(e^{j\omega}) - 0.5\omega$$

## Q-Shift Filters Design

- Fulfill the phase condition only approximately
- $\Rightarrow$  Only approx. shift independent
- Group delays  $\simeq \frac{1}{4}$  and  $\frac{3}{4}$  of a sample period



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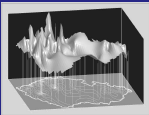
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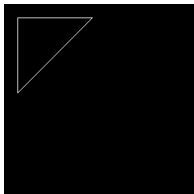
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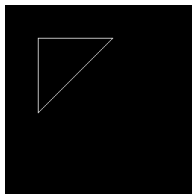
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## Approximate Shift Invariance

(a) ORIGINAL IMAGE



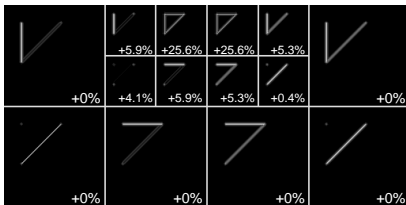
(b) AFTER THE SHIFT



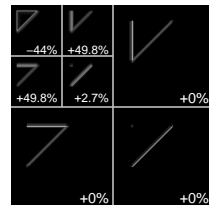
(c) CHANGE OF SUBBAND ENERGY

	DTCWT	DWT
level 1	0 %	0 %
level 2	4.5 %	34.1 %
level 3	5.7 %	118.8 %
level 4	6.2 %	77.6 %
level 4 (LoLo)	27.7 %	95.7 %

(d) 2-LEVEL DTCWT AFTER THE SHIFT

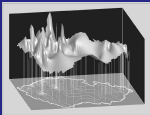


(e) DWT AFTER THE SHIFT



Percentual changes of subband energy.





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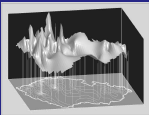
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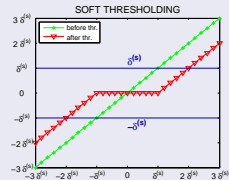
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## Denoising

- Computed Tomography (CT) images
- Suppressing lower energy wavelet coefficients (noise)
- Soft universal wavelet shrinkage

## Soft Thresholding

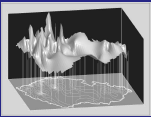


- Thresholding magnitudes of complex coefficients
  - Vary slowly
  - Not distorted by aliasing
- Signal to noise ratio [dB]

$$SNR = 20 \cdot \log_{10} \frac{l_{max} - l_{min}}{\hat{\sigma}_n}$$

$l_{max}, l_{min}$  ... max. and min. pixel value, resp.

$\hat{\sigma}_n$  ... noise standard deviation estimate (from areas - no image component)



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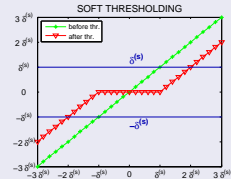
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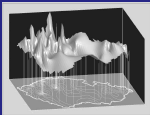


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## Median Absolute Deviation (MAD)

- Noise standard deviation estimator (for 1D signal)

$$\hat{\sigma}_{(mad)} = \frac{\text{median}\{|W_{1,0}|, |W_{1,1}|, \dots, |W_{1,N/2-1}|\}}{0.6745}$$

where  $W_{1,l} \dots l$ -th wavelet coefficient of level 1

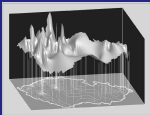
- Smallest scale w. coefficients - noise dominated
- For independent identically distributed Gaussian noise
- Robust against large deviations  $\Rightarrow$  noise variance

## Donoho Threshold

- Donoho soft universal threshold

$$\delta^{(s)} = \sqrt{2 \hat{\sigma}_{(mad)}^2 \log(N)}$$

where  $N$  is no. coefficients



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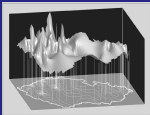
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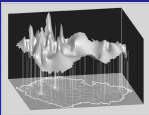
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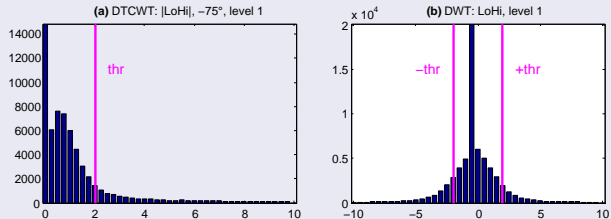
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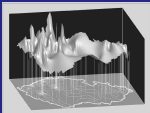
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## Histograms of Wavelet Coefficients



4 levels, 14-tap filters: Daubechies for DWT and q-shift for DTCWT



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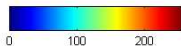
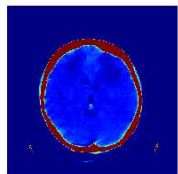
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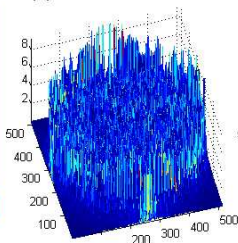
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## Residuals After Denosing

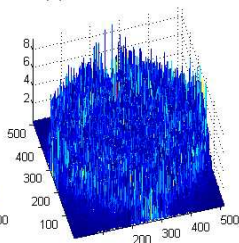
(a) ORIGINAL CT IMAGE



(b) DTCWT: RESIDUALS

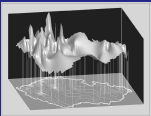


(c) DWT: RESIDUALS



Axial brain CT image.





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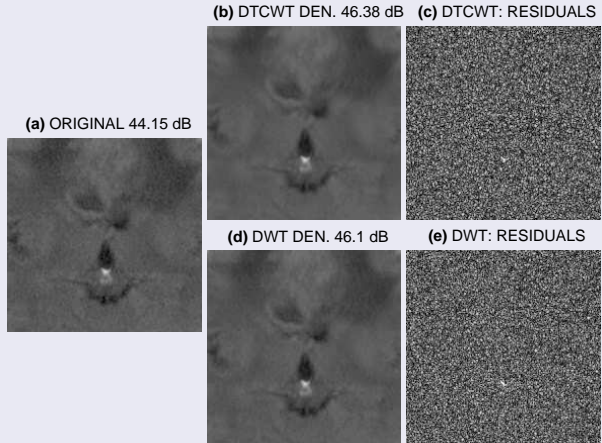
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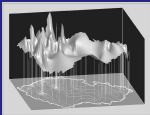
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## CT Image Denosing (Cuts)



Donoho universal soft threshold with MAD estimate.  
Similar SNR results for 2- and 3-level decomposition.



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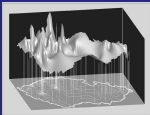
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## DTCWT surpasses DWT

- Shift dependence (reduced aliasing)
- Directional selectivity
- No zero-crossing of the coefficients at a singularity

## Future Study

- DTCWT in biomedical image denoising and enhancement
- Probability distribution of noise and of its wavelet coefficients in these images
- Wavelet shrinkage techniques



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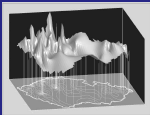
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